



## SHORT COMMUNICATION

# Drastic Increase in Nitric Oxide Content in Rat Brain under Halothane Anesthesia Revealed by EPR Method

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**ABSTRACT.** A drastic increase in nitric oxide (NO) content was revealed by the EPR method in rat brain cortex and cerebellum under halothane anesthesia. The NO scavenger diethyldithiocarbamate sodium salt (DETC) and ferrous citrate were injected into adult rats 30–60 min before anesthesia. Rats were anesthetized by inhalation of a halothane–oxygen mixture (1%, 1.5%, 2%, or 4%). After different times of anesthesia, rats were decapitated, and brain cortex and cerebellum were dissected, frozen in liquid nitrogen, and subjected to EPR spectroscopy. The concentration of NO was determined from the NO–Fe–DETC radical spectrum. In control animals, NO content in the cerebellum was only 68% of that in the cortex. We observed a time-dependent increase in NO content in the cortex and cerebellum of rats anesthetized with 1.5% halothane. In brain cortex, the NO level increased to six times that of waking animals after 30 min and remained at this level up to 60 min of anesthesia. In cerebellum the changes were less drastic, the NO level showing only a 2-fold increase. The same effect was produced by 1% and 2% halothane. Ketamine, chloral hydrate, and pentobarbital were used as reference drugs. None of these anesthetics produced effects similar to those of halothane. In ketamine-anesthetized rat brain, the NO content slightly decreased. Pentobarbital and chloral hydrate produced an insignificant increase in NO. Data are discussed in the context of possible interference of halothane in the regulation of nitric oxide synthase activity. BIOCHEM PHARMACOL 58;12:1955–1959, 1999. © 1999 Elsevier Science Inc.

**KEY WORDS.** spin trapping; nitric oxide; anesthetics; halothane

NO<sup>†</sup> plays a wide variety of roles in the central nervous system [1]. It was discovered recently that NO is a neurotransmitter (see [2] for review), and it is known to mediate NMDA receptor-associated neurotoxicity (see [3, 4] for review). Very early, it was supposed that halothane, one of the most widely used anesthetics, interferes with the action of NO. Inhibitors of NOS acted synergistically with halothane and decreased the MAC for anesthetics [5]. It was postulated that halothane depresses neurotransmission by L-glutamate and NMDA, thereby inhibiting NO production from the vascular endothelium, and decreases cyclic GMP content in brain. There is evidence of the direct action of halothane on NOS and NO production obtained in simple model systems [6, 7]. More detailed studies revealed that halothane suppressed NMDA-stimulated formation of cyclic GMP [8, 9]. Numerous biochemical and

pharmacological studies have attempted to explore the fine mechanisms of inhibition of NO-mediated neurotransmission by halothane [10, 11]. The results of these investigations, however, appear to be extremely contradictory [12, 13]. Study of halothane effects on NOS gene expression revealed an up-regulation, but no down-regulation, as one would expect [14]. The interference of halothane with NOS inhibitor action at the physiological level seems to be evident to some researchers [15], but others consider it extremely complicated and to involve many factors [16]. Halothane by itself produces vasodilatation of brain blood vessels [17, 18] and brain hyperemia [19].

In our opinion, direct measurements of NO in brain of organisms under anesthesia were necessary to clarify the situation. Therefore, we undertook a study of NO production in rat brain during halothane anesthesia. NO production was measured by an EPR method elaborated by Vanin *et al.* and others [20–22]. This method is based on the trapping of NO in a stable complex with iron ion and DETC and detecting its spectrum by means of EPR spectroscopy. The approach has been widely used for NO detection in different systems, including mammal brain tissues [20–25].

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<sup>†</sup> Abbreviations: NO, nitric oxide; NOS, nitric oxide synthase; DETC, diethyldithiocarbamate sodium salt; NMDA, N-methyl-D-aspartate; and MAC, minimal alveolar concentration.

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## MATERIALS AND METHODS

### Chemicals

DETC, ferrous sulfate, and sodium citrate were from Sigma. Halothane was purchased from Laboratories Belamont. Ketamine was from Alfasan. Xylazine was from Dopharma. Sodium pentobarbital was from Veterinaria AG. Chloral hydrate was from Fluka.

### Animal Treatment and Anesthesia

Animals were purchased from Grindex. All manipulations with animals were performed according to Latvian legislation. Male Wistar rats weighting 200–300 g were used in experiments. They were anesthetized either by inhalation of halothane in oxygen (1; 1.5; 2; 4%), using the Cyprane Fluotec rodent ventilator (Cyprane Ltd.), or by intraperitoneal injections of ketamine (100 mg/kg) with myorelaxant xylazine (5 mg/kg), pentobarbital (60 mg/kg), or chloral hydrate (300 mg/kg). In order to keep body temperature constant during anesthesia, the animals were placed on a heated support. The body temperature during narcosis was constantly monitored with a rectal thermometer. The gas flux was kept constant throughout the administration of halothane.

### Administration of Spin Trap Agents

To determine NO content in brain tissue, we used the protocol originally elaborated by Vanin *et al.* [20] and later modified for peculiarities of brain tissue [23]. Rats were injected intraperitoneally with 400 mg/kg of the NO scavenger DETC and ferrous citrate (40 mg/kg ferrous sulfate + 200 mg/kg sodium citrate subcutaneously) 30–60 min before decapitation.

### Sacrifice, Brain Dissection, and Sample Preparation

After the animals had remained under anesthesia for the required time, they were decapitated. Brains were removed and cooled at  $-20^{\circ}$  for 3 min. Brain cortex and cerebellum were dissected. Brain tissue was extruded through a 3-mL plastic syringe to a glass tube (2.5 mm in diameter, 30 mm in height), frozen in liquid nitrogen, and subjected to EPR spectroscopy. We used standard tubes with fixed volume that were always completely filled with tissue slurry, which enabled us to standardize the amount of tissue used in our experiments. Samples were prepared rapidly without any delay, which also enabled us to standardize the time taken to prepare samples, which was equal for all samples (10 min).

### EPR Measurements

Tubes with samples were placed in EPR spectrometer quartz duar. Relative NO content in the samples was evaluated by comparing the intensity of the NO signal with a standard

signal intrinsic to the duar. EPR spectra were recorded in liquid nitrogen using the EPR spectrometer Radiopan SE/X2544. Conditions of EPR measurements were: 2.5 mW microwave power, 9.24 GHz microwave frequency, 100 kHz modulation frequency, 0.4 mT modulation amplitude, and  $2.5 \times 10^5$  receiver gain.

### Statistical Analysis

Significance of differences between the groups (waking animals and animals under anesthesia, or groups differing in concentration of anesthetic or time under anesthesia) was evaluated according to Student's *t*-test ( $P < 0.05$ ).

## RESULTS AND DISCUSSION

Figure 1 presents the spectra of NO in rat brain tissues. The spectra all have a typical shape of the Cu–DETC spectrum with a superposed NO peak. The intensity of the Cu–DETC spectrum indicates the bioavailability of the tissue under study to DETC. We regarded the height between the maximum of the peak at  $g = 2.047$  and the trough at  $g = 2.025$  as the size of the NO–Fe–DETC signal ( $I_0$ ) [25]. Our spectra reproduce very well previously published spectra of NO–Fe–DETC in brain tissues [20–25]. To determine the background NO level in rat brain, rats were injected with the NO scavenger DETC and ferrous citrate and sacrificed 30 min later. The average signal intensity in the cortex of these animals will be referred to as 100% for further determinations ( $100 \pm 37$ ;  $N = 15$ ). NO content in cerebella of animals from the same group was lower,  $68 \pm 19$ ;  $N = 15$ . In measurements made after longer time intervals following scavenger administration (45 or 60 min), the intensity of the NO signal remained within the same range after 45 and 60 min ( $100 \pm 31$ ;  $N = 6$  and  $146 \pm 80$ ;  $N = 6$ , respectively). After a shorter time (15 min) the signal was very weak albeit detectable. These differences must have been due to DETC pharmacokinetics and, in order to avoid their influence in our experiments, we determined NO content in brain within a time range of 30 and 60 min after DETC administration.

To study the influence of halothane anesthesia on NO content in rat brain, rats were anesthetized with 1.5% halothane. Animals were sacrificed at different time intervals after starting narcosis. The NO scavenger was injected 60 min before decapitation. After 5 min of narcosis, the NO content in brain cortex had already doubled and by 30 min it had increased six-fold, remaining at this level for up to 60 min of anesthesia. The difference in the EPR spectra of waking and halothane-anesthetized animals is clearly seen in Fig. 1 (compare spectra *a* and *e*, *a'* and *e'*): the height between the maximum peak at  $g = 2.047$  and the trough at  $g = 2.025$  as the size of ( $I_0$ ) is six times more intensive in the cortex preparation of halothane-anesthetized rats (*e*) than that of waking rats (*a*). In Fig. 2, data are presented in quantitative form.

The dependence of NO content in brain cortex on

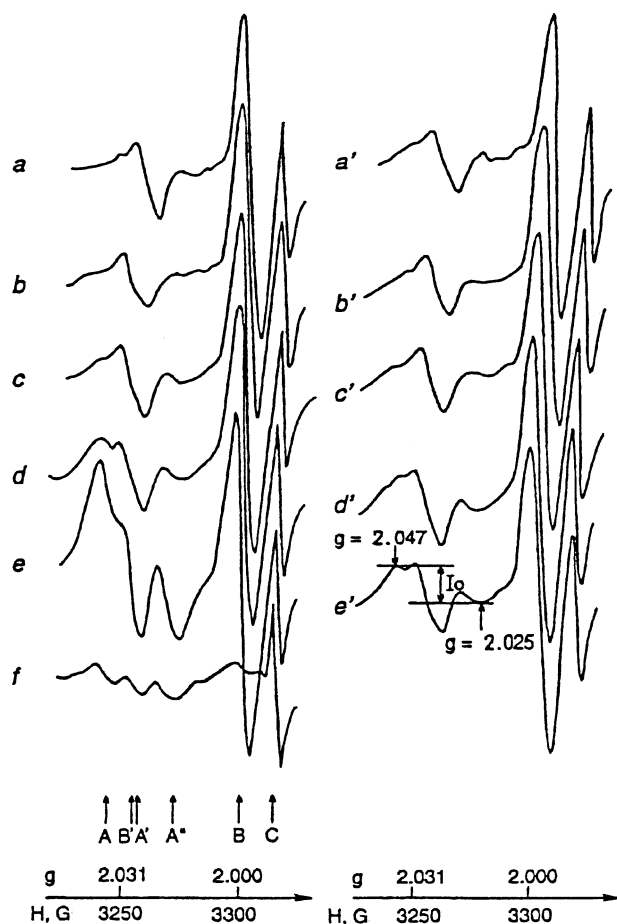


FIG. 1. EPR signals obtained from the brain cortex (a-e) and cerebellum (a'-e') during various anesthetic regimens: a, a'-waking animals; b, b'-ketamine (100 mg/kg, 30 min); c, c'-chloral hydrate (300 mg/kg, 30 min); d, d'-pentobarbital (60 mg/kg, 30 min); e, e'-halothane (1.5%, 30 min), f-NO-Fe-DETC signal without Cu-DETC signal. A, A', A': signals from the NO-Fe-DETC complex; B, B': signals from Cu-DETC complex; C: standard signal. Conditions of EPR spectroscopy: 2.5 mW microwave power, 0.4 mT modulation amplitude, 9.24 GHz microwave frequency, and 100 kHz modulation frequency,  $2.5 \times 10^5$  receiver gain. All rats were administered with DETC (400 mg/kg) ferrous citrate (40 mg/kg  $\text{Fe}_2\text{SO}_4$  + 200 mg/kg sodium citrate subcutaneously) 60 min before decapitation. g = g factor and H = tension of magnetic field.

halothane concentration was evaluated in animals subjected for 45 min to different concentrations of anesthetic. Anesthesia with 1% halothane increased NO content up to  $669 \pm 166$ ; N = 10, and 1.5% and 2% halothane raised it to  $585 \pm 105$ ; N = 11 and  $546 \pm 51$ ; N = 6, respectively. Apparently, in this range of concentrations, NO content in brain cortex does not depend on halothane concentration, as differences in NO content are not statistically significant. We were not interested in lower concentrations, as the lowest of the studied concentrations was close to MAC for halothane (0.7%) and a decrease in the anesthetic concentration made it difficult to achieve narcosis.

Time was necessary to obtain a significant increase in NO content. After 1 min of anesthesia, there was only a

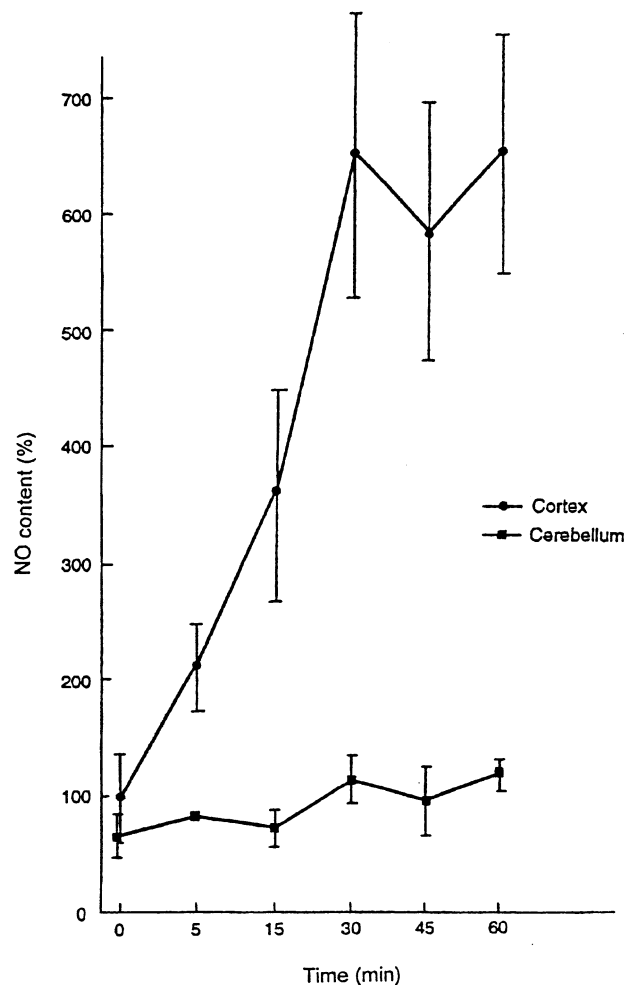


FIG. 2. Nitric oxide content in rat brain cortex and cerebellum during development of halothane anesthesia (1.5%). Data shown are the means  $\pm$  SD, N = 4-15. Abscissa: time, minutes; ordinate: NO content, percentage of the mean value in the cortex of waking animals.

tendency for NO increase in the cortex ( $131 \pm 44$ ; N = 14), although a high concentration of halothane (4%) was applied to achieve anesthesia in this short time interval. In cerebellum, halothane anesthesia produced less pronounced changes in NO content. After 1-min anesthesia produced by 4% halothane, the increase in the NO content was not yet significant,  $76 \pm 16\%$ ; N = 5 compared to  $68 \pm 19$ ; N = 15. During anesthesia with 1.5% halothane, a 1.5-fold increase in NO content was achieved within 30-60 min (Fig. 2). The effect was more pronounced with higher concentrations of anesthetic: after 45 min with 2% halothane, NO in cerebellum rose to  $271 \pm 32$ ; N = 3. Thus, halothane anesthesia produces a drastic increase in NO content in brain cortex and a similar, although less pronounced, effect in cerebellum. In order to elucidate whether this effect was due to the drug action or the result of the anesthesia itself, we compared the action of halothane with that of other anesthetics with different chemical structures and mechanisms of action.

**CHLORAL HYDRATE.** Under chloral hydrate action, NO increased slightly in brain cortex 30 min after administration ( $178 \pm 49$ ;  $N = 4$ ). No effect was detected in cerebellum ( $55 \pm 8$ ;  $N = 4$ ).

**KETAMINE.** After 30 min, ketamine action did not produce any changes in NO content in the cortex ( $102 \pm 8$ ;  $N = 4$ ) and manifested a tendency to decrease 30 min later ( $51 \pm 22$ ;  $N = 4$ ). In cerebellum, NO content remained unchanged 30 min after ketamine administration ( $70 \pm 26$ ;  $N = 4$ ), decreasing 30 min later ( $45 \pm 5$ ;  $N = 4$ ).

**PENTOBARBITAL.** Anesthesia with this barbiturate slightly increased the NO content in brain cortex ( $137 \pm 12$ ;  $N = 3$ ) and cerebellum ( $84 \pm 15$ ;  $N = 3$ ).

Thus, during anesthesia produced by three different reference drugs, we did not observe any drastic increase in NO-Fe-DETC formation during halothane action. We conclude that halothane greatly increases NO content in brain. This effect is apparently due to an increase in NO production rather than to an accumulation of the NO-Fe-DETC complexes over time. In models similar to ours, a rapid decline in the signal intensity has been observed in the course of brain ischemia [22]. This would not be possible if the complexes were accumulated in the brain. It should be pointed out that the observed increase in intensity of the NO-Fe-DETC complex EPR spectrum indeed reflects changes in NO concentration in rat brain. Although some reports indicate that the Fe-DETC complex can reduce nitrite to nitric oxide [26], it is unlikely that the Fe-DETC complex can interact with charged nitrite in living tissue, as the complex is highly hydrophobic and compartmentalized in biomembrane fraction. Special studies [27] confirm this point of view. The increase in the EPR signal in rat brain under halothane anesthesia might also be due to an increase of Fe-DETC accessibility to NO under action of the drug. Although difficult to test experimentally, this hypothesis seems to be unlikely. We suggest that either halothane acts as a catalyst of the complex formation—and this hypothesis has no chemical background—or that it facilitates DETC transport to the brain. In the latter case, we should have observed a stronger signal in cerebellum, since it contains more neuronal NOS [2]. Moreover, it was shown that under experimental conditions analogous to ours, the Fe-DETC trap was nearly equally distributed throughout the body and was not a limiting factor for the trapping of NO under either basal or stimulated conditions [28]. DETC concentration in tissues is 20- to 200-fold higher than NO concentration [29]. Cu-DETC spectra in our experiments also indicated that we had a large excess of Fe-DETC complex over NO. Possible modification of blood-brain barrier permeability during narcosis also cannot change much Fe-DETC concentration in brain, as even osmotic disruption of the barrier did not influence it [30].

We believe that together with indirect data indicating involvement of NO production in halothane action [17, 19,

31–33] our results indicate increased production of NO under halothane anesthesia. The mechanism of the observed phenomenon is still to be elucidated. Halothane might activate NOS directly, as has been observed in some studies [9]. The observed increase in NO concentration in brain tissue might also be due to activation of endothelial NOS, as halothane possesses a vasodilating effect that is mediated by endothelial NOS [17, 19, 32, 34, 35]. Disturbance of energy metabolism in brain under halothane action [36–39] can provoke ischemization of brain tissues and trigger NO production [22–25]. Our data comparing the action of several anesthetics are consistent with previous reports of an attenuation of the increase in arterial pressure provoked by NOS inhibitors under halothane narcosis, a phenomenon that is not observed under the action of other anesthetic agents (ketamine, barbiturates, isoflurane, and others) [40, 41]. In this case, increased NO content under halothane anesthesia should have equilibrated the decrease in NO production due to action of the NOS inhibitor, as other anesthetics could not produce this effect.

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